



Automated Phantom Analysis for Gamma Cameras - An Efficient, Accessible, Consistent, and Sensitive Method for Quality Control

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BUILDING BRIDGES. CULTIVATING SAFETY. GROWING VALUE.

Disclosures and Disclaimers

Funding for this project was provided by Atirix Medical Systems

- Atirix sells the QC-Track[®] system for imaging QC
- All analysis was performed in QC-Track[®]



Contributors:

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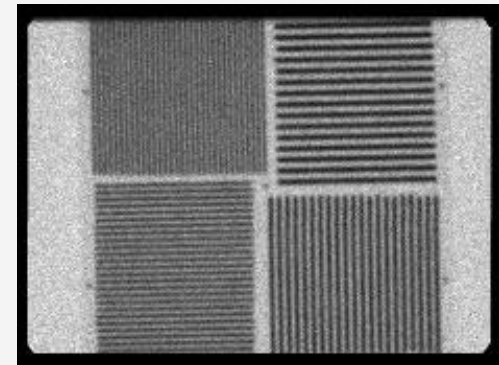
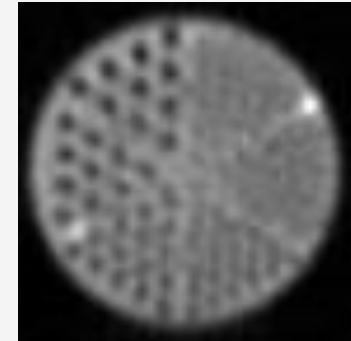
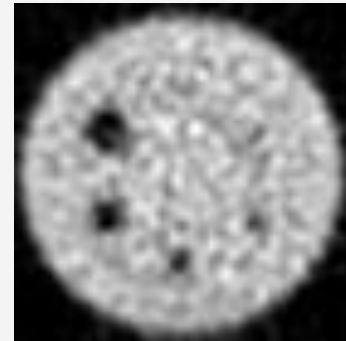
Why strive for excellence in Quality Control?

- Maintain high quality images
 - Better diagnostic capabilities
 - Better patient care
- Higher sensitivity to system degradation
 - Catch system failures early
 - Reduce imaging downtime
- ACR/TJC/State Regulation compliance
- Trend towards stricter QC requirements for all modalities
 - Stay ahead of the curve

Clinical Nuc Med QC Methods

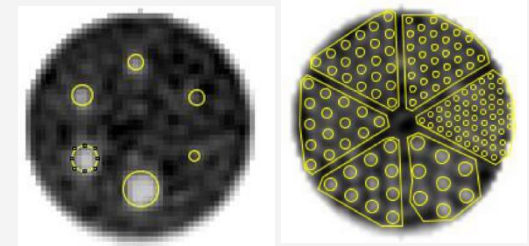
- Most hospitals and clinics
 - Visual assessment of image quality
 - Discrete levels of assessment
 - Subject to individual bias and inconsistencies

- Research/academic environments
 - Quantitative analysis in ImageJ, MATLAB, or in-house software
 - Larger image acquisition matrix (longer scan time, more disk space) sometimes required

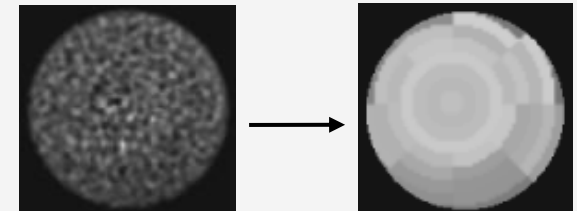


Existing methods for Quantitative Phantom Analysis

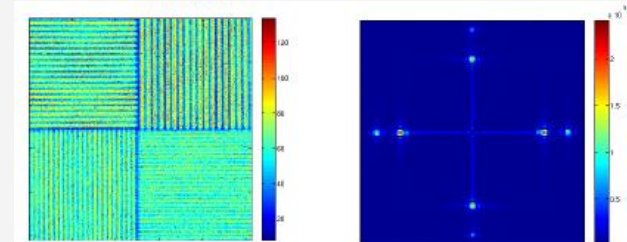
- Hirtl et. al. – ImageJ plugin
 - Spheres and rods (contrast)
 - Uniformity (Hough transform)
- Madsen
 - Uniformity analysis (annular sampling)
- Nijs et. al. – MATLAB scripts
 - Bar phantom (Fourier analysis)
- DiFilippo
 - ROC curve (rods), SNR, noise texture



Hirtl. et al. Med Phys. 44 (5), May 2017



Madsen. Med Phys. 24 (11), Nov 1997



De Nijs et. al. J Phys. Conf. Ser. 317 (1), Sept 2011

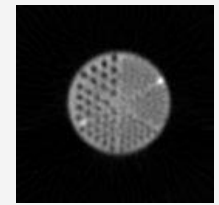
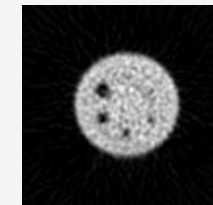
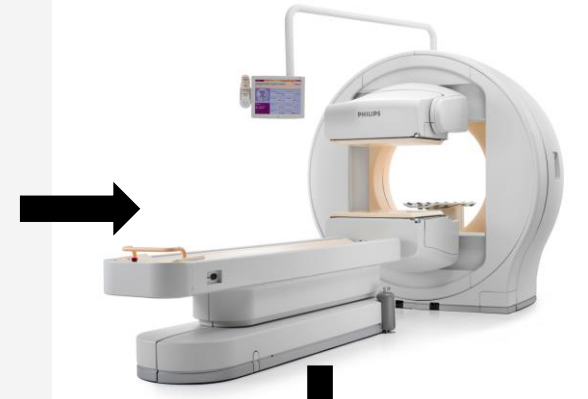
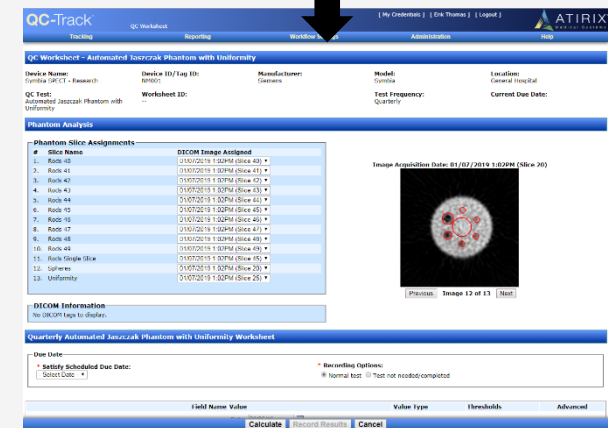
Main drawbacks: computationally expensive and complex methods, ImageJ/MATLAB workflow unlikely in clinical setting

Objective

- Provide method that exceeds visual analysis
- Sensitive and objective
 - Simple computations
- Focus on areas where automation is limited clinically
 - ACR/Jaszczak Phantom
 - Bar phantoms
- Easily accessible to clinics (technologists)
- Incorporate into QC-Track, a centralized database for QC
- Simple QC workflow = less downtime

Clinical Workflow

- Acquire Images using Standard QC protocols
- ‘For presentation’ images uploaded to QC-Track via DICOM send
 - ROIs drawn and calculations performed automatically
- Results stored in a database on a local (on-site) network server
- For research purposes, results were exported from QC-Track and analyzed in Excel

QC-Track
QC Worksheet - Automated Jaegerzrak Phantom with Uniformity

Device Name: Gamma QC T - Research Device ID / Tag ID: 88100 Manufacturer: Gamma Model: Gamma Location: General Hospital

QC Test: Automated Jaegerzrak Phantom with Uniformity Worksheet ID: Test Frequency: Quarterly Current Date:

Phantom Analysis

#	ROI Name	DICOM Image Assigned
1.	Rock 40	21072019 1 10PM (Slice 40) ▾
2.	Rock 41	21072019 1 10PM (Slice 41) ▾
3.	Rock 42	21072019 1 10PM (Slice 42) ▾
4.	Rock 43	21072019 1 10PM (Slice 43) ▾
5.	Rock 44	21072019 1 10PM (Slice 44) ▾
6.	Rock 45	21072019 1 10PM (Slice 45) ▾
7.	Rock 16	21072019 1 10PM (Slice 46) ▾
8.	Rock 17	21072019 1 10PM (Slice 47) ▾
9.	Rock 48	21072019 1 10PM (Slice 48) ▾
10.	Rock 49	21072019 1 10PM (Slice 49) ▾
11.	Rock Single Slice	21072019 1 10PM (Slice 45) ▾
12.	Spheres	21072019 1 10PM (Slice 25) ▾
13.	Uniformity	21072019 1 10PM (Slice 25) ▾

DICOM Information
No DICOM tags to display.

Quarterly Automated Jaegerzrak Phantom with Uniformity Worksheet

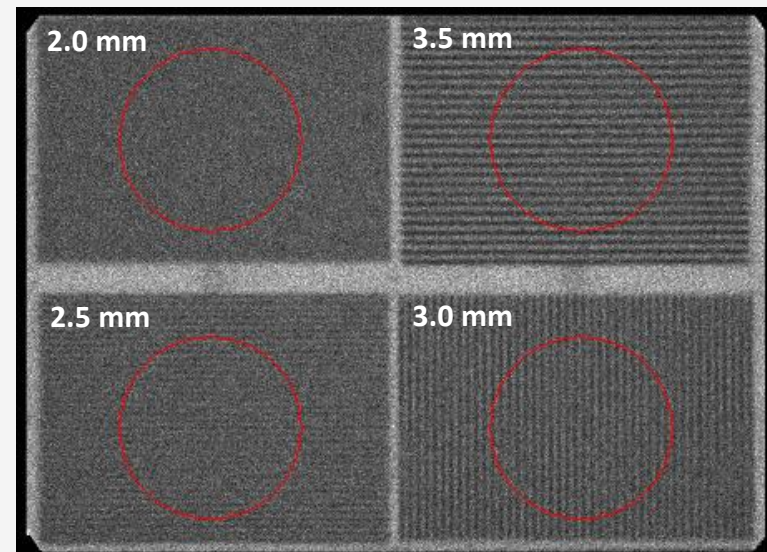
Date Date: Satisfy Scheduled Date: Reordering Options: Normal test Test not possible-completed

Field Name Value Value Type Threshold Advanced

Calculate Second Results Cancel

Four-Quadrant Bar Phantom

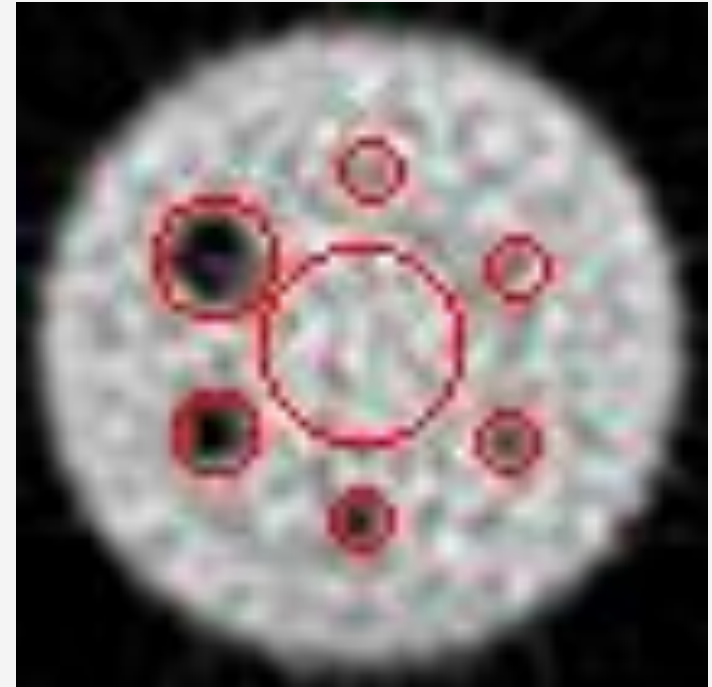
- Goal: assess the spatial resolution of a planar gamma camera scan by determining “smallest spacing without aliasing”
- Automated Method:
 - Software places circular ROIs in each quadrant based on phantom center
 - Calculates standard-deviation based modulation transfer function (MTF) as described by Hander et. al.



Hander TA et. al. An improved method for rapid objective measurement of gamma camera resolution. *Med Phys.* 2000; 27:2688:2692.

Jaszczak Phantom Spheres Section

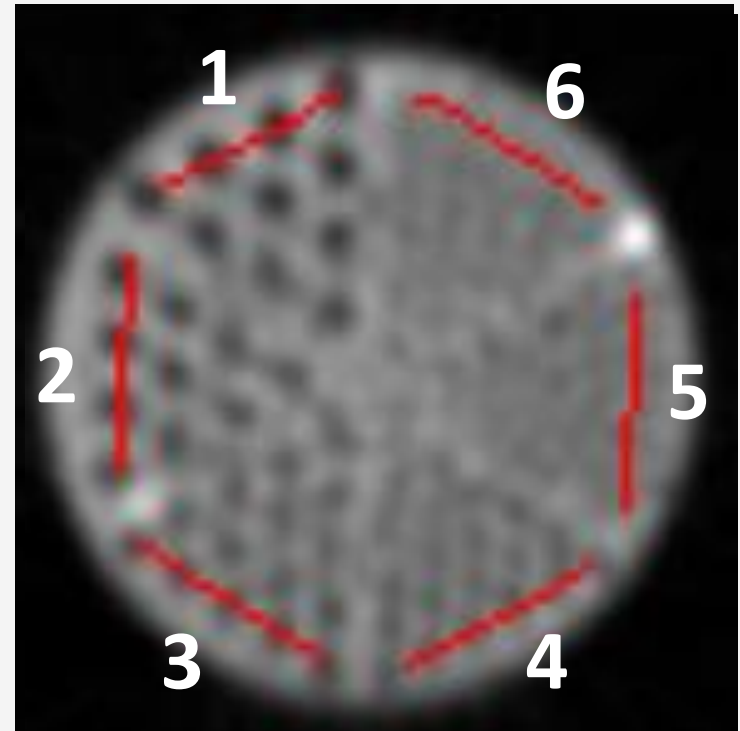
- Goal: assess the contrast of a SPECT scan by determining “limiting observable sphere”
- Automated Method:
 - Software places circular ROIs around each sphere
 - Calculates contrast-to-noise ratio (CNR) for each sphere



Method adapted from AAPM Report 52: Quantitation of SPECT Performance. Med Phys. 22 (4), April 1995

Jaszczak Phantom Rods Section

- Goal: assess the spatial resolution of a SPECT scan by determining “limiting set of rods”
- Automated Method:
 - Software automatically places line ROIs on each rods section
 - Calculates basic modulation using pixel values within line ROI



Jaszczak Phantom Uniformity Section

- Goal: assess the uniformity of a SPECT scan
- Automated Method:
 - Compare mean counts in top, right, bottom, and left ROIs to mean counts within center ROI
 - Similar to Daily GE Water phantom and CATPHAN Module 486 (CT)

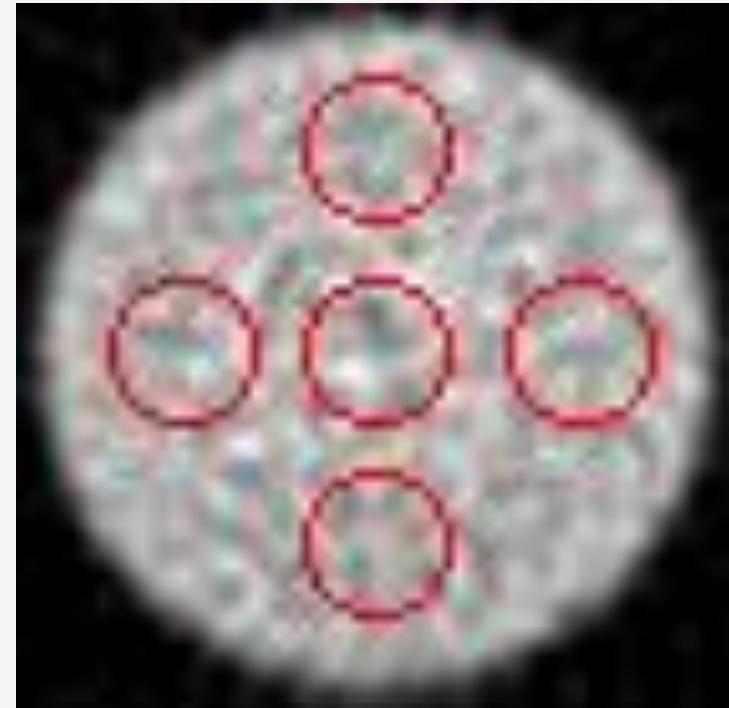
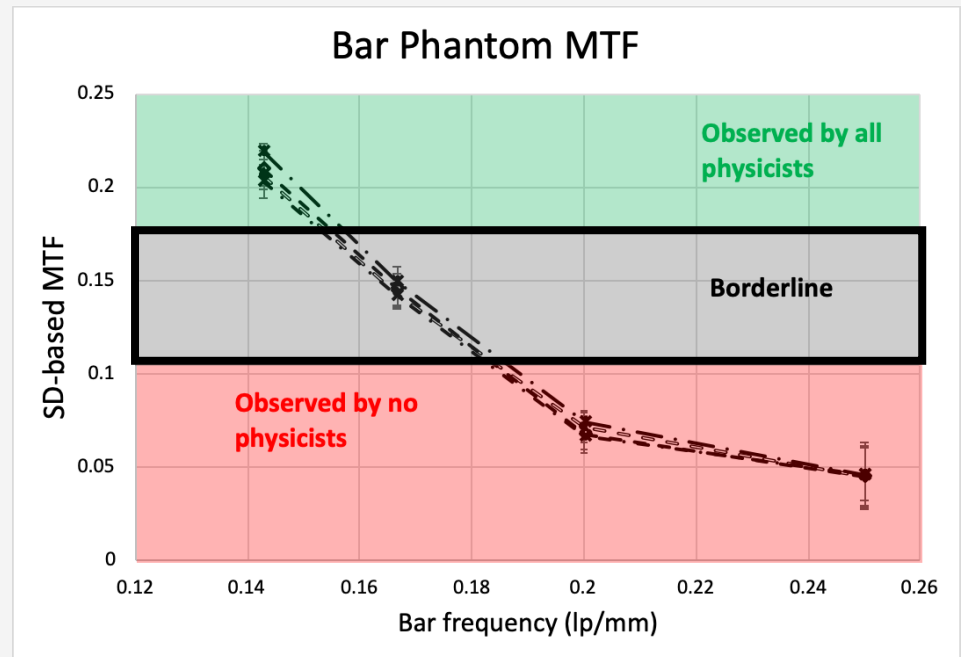


Image Acquisition and Study Details

- Imaging units
 - 3 SPECT units
 - 1 Older model
 - 1 SPECT/CT unit
- Images
 - Analyzed previously captured images to build phantoms and worksheets within QC-Track
 - After clinical implementation, acquired data over 6-7 months using standard ACR, vendor, or physicist protocols
 - Bar phantom – weekly (200+ images over 4 imaging units)
 - Jaszczak phantom – quarterly (8+ images over 4 imaging units)

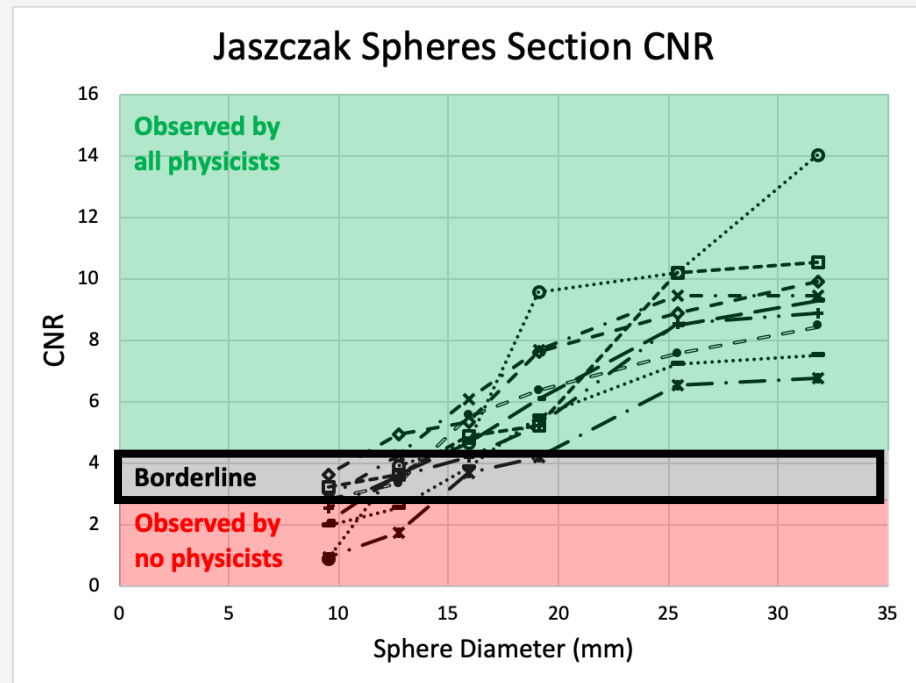
Four-Quadrant Bar Phantom Results

- Analysis of roughly 40 acquisitions each over 4 scanners
- MTF values for each bar width show consistency over many acquisitions
- Physicists visual assessment showed disagreement
 - borderline region between 0.1-0.18 MTF
- Interpolation of curve allows for more continuous assessment of image quality



Jaszczak Phantom Spheres Section Results

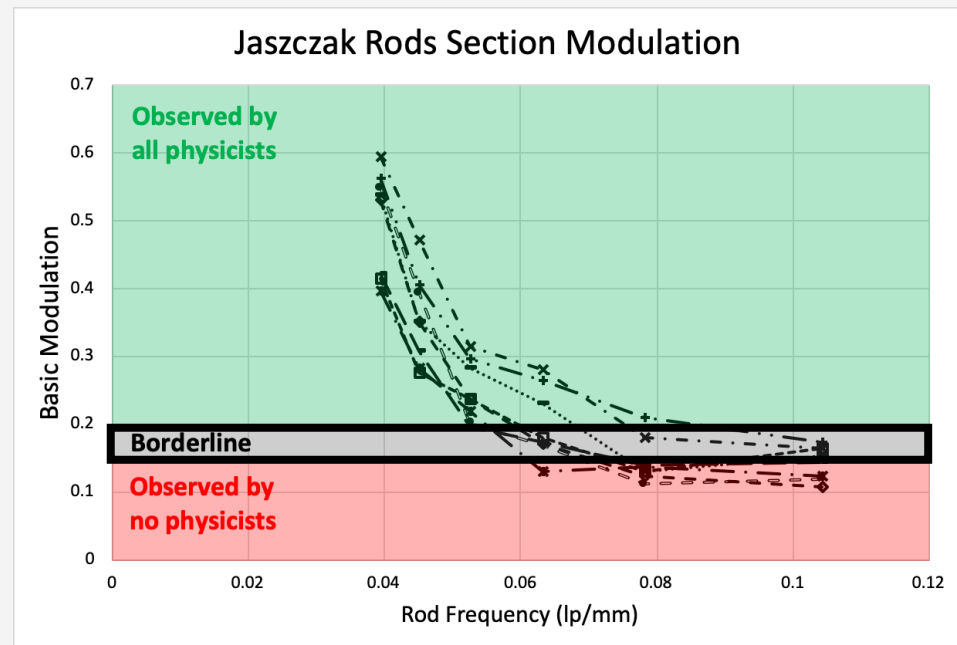
- CNR analysis over 9 tomographic reconstructions of Jaszczak phantom
- In general, CNR increases with sphere size
- Results more variable due to image variability
- Physicist visibility correlates well with previous guidelines (CNR > 3-5 for visible objects)*



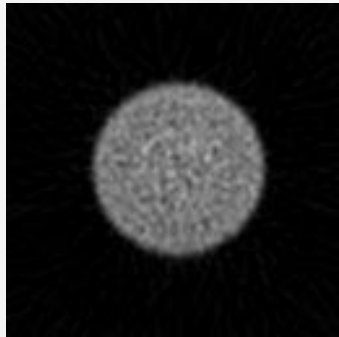
*Cherry. et al. Phys in Nuc Med, 4e. p244, 2012

Jaszczak Phantom Rods Section Results

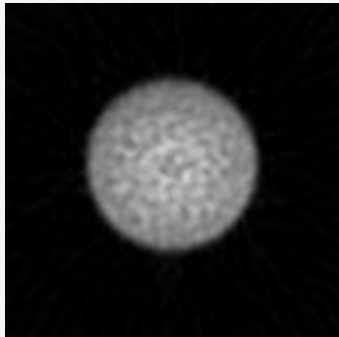
- Modulation analysis over 10 slices each of 9 acquisitions of the Jaszczak phantom
- Modulation curve shape
 - Decreasing until higher frequencies (noise level)
- Physicist visual read shows distinct areas where visual assessment suffices but also borderline regions where biases come into play



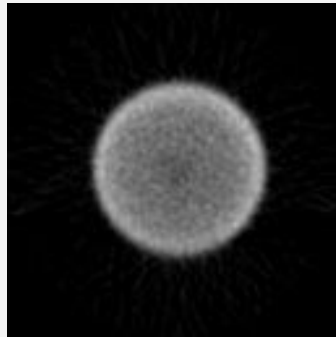
Jaszczak Phantom Uniformity Section



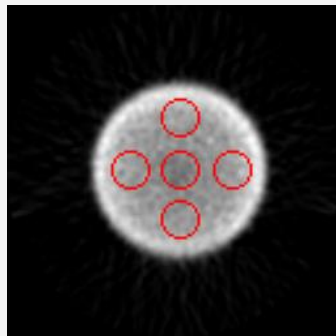
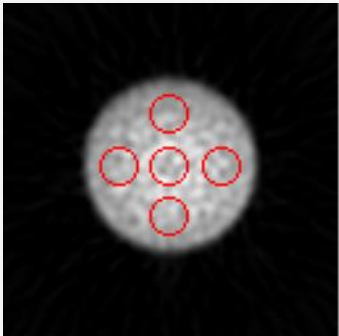
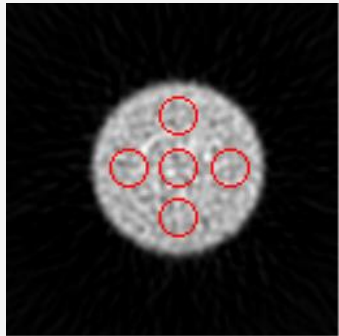
Acquisition 1



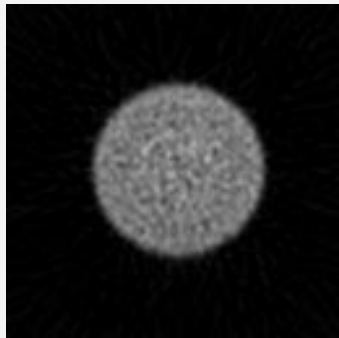
Acquisition 2



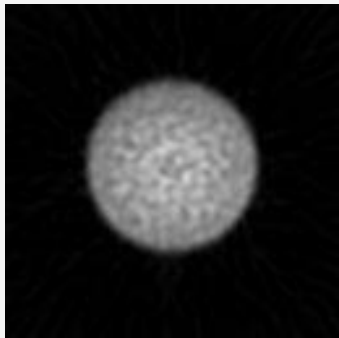
Acquisition 3



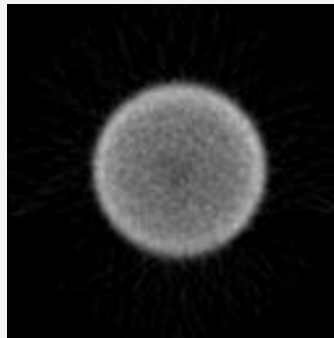
Jaszczak Phantom Uniformity Section



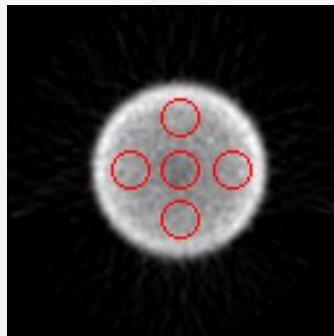
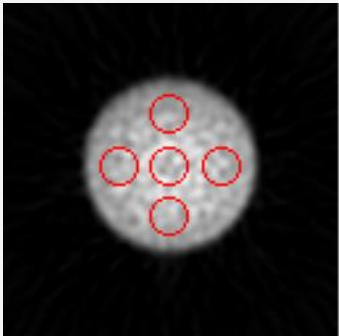
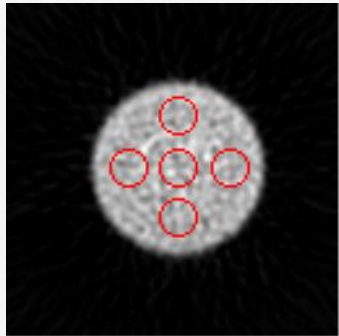
Acquisition 1



Acquisition 2



Acquisition 3



Acquisition	Greatest % deviation
1	-5.88 %
2	-15.1 %
3	27.5 %

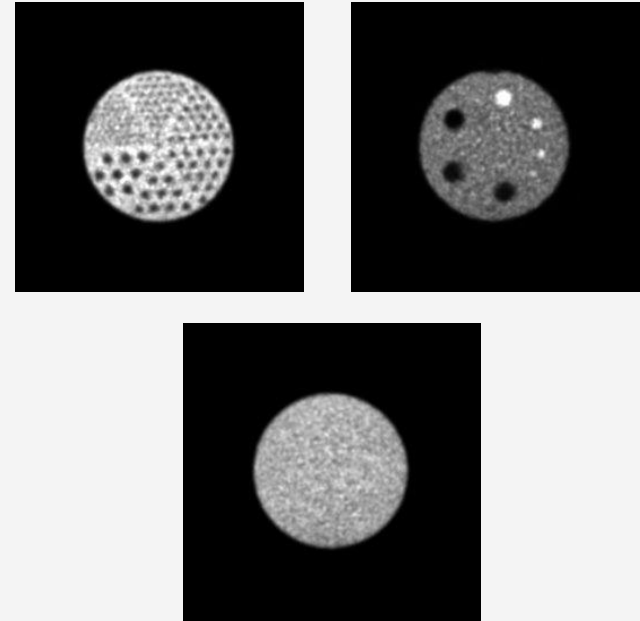
Conclusions

- Our framework can be used in clinical settings
 - Simple yet quantitative
 - Accessible to technologists
 - Easy to incorporate into workflow
- Automated method can be used to detect QC situations that may be overlooked during visual analysis
 - Allows more sensitive tracking of image quality parameters with quantitative thresholding

Future Work

- Analysis of PET phantoms
 - Rods
 - Specific uptake value and contrast detectability
 - Uniformity

- Incorporate noise texture analysis for more robust uniformity assessment



Thank you!

Extra Slides (1/6) – Full Acquisition Parameters

Acquisition Parameters- Planar Bar Phantom	
Isotope	Co-57
Total Counts	5,000,000
Energy Window	+/-20% centered on 122 keV
Collimator	Low Energy High Resolution (LEHR)
Matrix Size	256x256
Zoom Factor	1

Acquisition Parameters- Jaszczak Phantom	
Isotope	Tc-99m
Injected Activity	10-15 mCi
Energy Window	+/-15% centered on 140 keV
Collimator	Low Energy High Resolution (LEHR)
Matrix Size	128x128
Zoom Factor	1.45
Acquisition	180° rotation, non-circular orbit
Number of Views	64
Time per View	~13 sec
Reconstructed Slice Thickness	3 mm
Reconstruction Algorithm	Filtered back projection
Attenuation Correction	Chang- 0.15 attenuation coefficient

Extra Slides (2/6) – Bar Phantom Analysis

ROI Size and Placement: 131.9 mm diameter circle ROI placed centrally within each bars section using geometric considerations.

$$MTF = \frac{\pi\sqrt{2}}{4 \cdot A(f_b, w_p)} \cdot \frac{\sqrt{\sigma_{ROI}^2 - \mu_{ROI}}}{\mu_{ROI}}$$

$$A(f_b, w_p) = \frac{\sin(\pi \cdot f_b \cdot w_p)}{\pi \cdot f_b \cdot w_p}$$

$$f_b = \frac{1}{2 \cdot (\text{bar width})}$$

Pixel size correction factor

w_p = pixel size

Bar Width (mm)	Bar Frequency (lp/mm)
3.5	0.143
3.0	0.167
2.5	0.20
2.0	0.25

Hander TA et al. (2000). An improved method for rapid objective measurement of gamma camera resolution. Medical physics. 27. 2688-2692.

Extra Slides (3/6) – Jaszczak Phantom Spheres Analysis

ROI Placement: Circle ROI, slightly larger than sphere, placed centrally over each sphere using manufacturer's geometric specifications.

$$\text{CNR} = \frac{|\mu_{\text{center}} - \text{min}_{\text{sphere}}|}{\sigma_{\text{center}}}$$

Adapted from:

AAPM Report 52: Quantitation of SPECT Performance. Medical physics. 22 (4), April 1995

Sphere diameter (mm)	ROI Diameter (mm)
31.8	42.8
25.4	29.7
19.1	23.0
15.9	19.7
12.7	19.7
9.5	19.7

Extra Slides (4/6) – Jaszczak Phantom Rods Analysis

ROI Placement: Line ROI 72mm in length placed centrally over outer set of rods in each section using manufacturer's geometric specifications.

$$\text{Modulation} = \frac{|\max_{\text{ROI}} - \min_{\text{ROI}}|}{\max_{\text{ROI}} + \min_{\text{ROI}}}$$

Rod diameter (mm)	Rod Frequency (lp/mm)
12.7	0.039
11.1	0.045
9.5	0.053
7.9	0.063
6.4	0.078
4.8	0.104

Extra Slides (5/6) – Jaszczak Phantom Uniformity

ROI Placement: Circle ROI, 50mm diameter, placed in center of phantom and at distance of 65mm from center in 4 directions (0°, 90°, 180°, 270°)

$$\% \text{ Deviation}_{\text{ROI},i} = \frac{\mu_{\text{ROI},i} - \mu_{\text{ROI,center}}}{\mu_{\text{ROI},i} + \mu_{\text{ROI,center}}} \times 100$$

Extra Slides (6/6) – Full References

- Hirtl, A. , Bergmann, H. , Knäusl, B. , Beyer, T. , Figl, M. and Hummel, J. (2017). Technical Note: Fully-automated analysis of Jaszczak phantom measurements as part of routine SPECT quality control. Medical physics. 44. 1638-1645. doi:10.1002/mp.12150
- Madsen, Mark. (1997). A method for quantifying SPECT uniformity. Medical physics. 24. 1696-700. doi:10.1118/1.597956.
- Vickery, A., Jørgensen, T., and Nijs, Robin. (2011). NEMA NU-1 2007 based and independent quality control software for gamma cameras and SPECT. Journal of Physics: Conference Series. 317. 012023. 10.1088/1742-6596/317/1/012023.
- Jaszczak RJ. Nuclear Imaging Phantom. United States: Patent No. 4,499,375; 1985.
- Data Spectrum Corporation. http://www.spect.com/pub/Flanged_Jaszczak_Phantoms.pdf. Accessed June 6, 2019.
- Hander TA et. al. (2000). An improved method for rapid objective measurement of gamma camera resolution. Medical physics. 27. 2688-2692.
- AAPM Report 52: Quantitation of SPECT Performance. Medical physics. 22 (4), April 1995
- Cherry S.R., Sorenson J.A., and Phelps M.E. (2012). Physics in Nuclear Medicine, 4e. Ch 15: Image Quality in Nuclear Medicine. p244.